## A Novel Photothermal Nanocrystals of $Cu_7S_4$ Hollow Structure for Efficient Ablation of Cancer Cells

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Abstract:  $Cu_{2-x}S$  nanocrystals (NCs), characterized by low cost, low toxicity, high stability and high photothermal conversion efficiency, provide promising platforms as photothermal agents. Herein, a novel two-step synthesis has been developed for  $Cu_7S_4$  nanocrystals with hollow structure using the as-prepared copper nanoparticles as starting a solid precursor followed by hot-injection of sulfide source. The  $Cu_7S_4$  NCs exhibit intense absorption band at Near-infrared (NIR) wavelengths due to localized surface plasmon resonance (LSPR) mode, which can effectively convert 980 nm-laser energy into heat. Moreover, the localized high temperature created by  $Cu_7S_4$  NCs under NIR irradiation could result in efficient photothermal ablation (PTA) of cancer cells *in vivo*, demonstrating a novel and promising photothermal nanomaterials.

Keywords: Semiconductor nanocrystals; Near-infrared absorption; Photothermal

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### Introduction

Near-infrared (NIR)-laser-driven photothermal ablation (PTA) therapy has attracted great attention in recent years as a minimally invasive and potentially more effective treatment alternative to conventional approaches [1-16]. In order to promote the photothermal conversion efficiency and gain access to efficient PTA therapy, it is the developing novel photothermal conversion agents that we are focusing on.Currently, four types of photothermal agents have been extensively developed in PTA therapy. The first type are organic compounds (e.g., indocyanine green (ICG) dye [1] and poly aniline nanoparticles [2]), which may suffer from limitations such as photobleaching or unsatisfactory photothermal conversion efficiency. The second type are carbon nanomaterials (including carbon nanotubes [3-5] and graphene [6-9]) whose absorption coefficient in the NIR region is usually not as high as expected. The third type are noble metal nanostructures, such as nanorods [10-12], nanoshells [13,14], nanocages [15,16], nanostars [17] and Pd- nanosheets [18].

These noble metal nanostructures exhibit intense NIR photoabsorption, and also are the most widely explored kind of photothermal agents. However, their practical applications are limited by the high cost. Alternatively, copper-containing semiconductor nanocrystals, characterized by low production cost, high stability, low toxicity, and high photothermal conver-

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sion efficiency, provide promising platforms as photothermal agents [19-23]. CuS nanoparticles [24], CuS superstructures [21], Cu<sub>9</sub>S<sub>5</sub>nanocrystals [19], and Fe<sub>3</sub>O<sub>4</sub>@Cu<sub>2-x</sub>S [22], Cu<sub>9</sub>S<sub>5</sub>@SiO<sub>2</sub> [20] nanocomposites have been developed as 980 nm laser-driven photothermal agents for efficient PTA of cancer cells *in vitro* and *in vivo*. To meet the severe requirements of future PTA therapy, it is still necessary to develop novel kind of copper chalcogenides based photothermal agents. Herein, we have developed a novel two-step method for preparation of Cu<sub>7</sub>S<sub>4</sub> nanocrystals with hollow structure and investigated them as a potential of 980 nm-laser-driven photothermal agents.

### Experimental

Characterization: Sizes, morphologies, and microstructures of the samples were determined by field emission transmission electron microscope (TEM, JEOL, JEM-2100F). Powder X-ray diffraction (XRD) was conducted by a D/max-2550 PCX-ray diffract meter (Rigaku, Japan). UV-Vis-NIR absorption spectra were measured on a UV-2550 Spectrophotometer (Shimadzu, Japan).

Synthesis of Cu<sub>7</sub>S<sub>4</sub> NCs: All of the chemicalswere bought from Aladdin and are analytically pure, which were used as received without further purification. The preparation of copper NCs followed a modified procedure [25]. Briefly, 0.5 mmol of copper acetylacetonate was dissolved in 15 mL of oleylamine in a 100 mL flask, which was purged with dry nitrogen gas to remove residual water and oxygen. The reaction mixture was heated to  $230^{\circ}$ C at a rate of  $5^{\circ}$ C /min by a heating mantle while being magnetically stirred and then kept at 230°C for 10 min to form copper NCs. Subsequently, a certain amount of sulfur (e.g. 0 mmol, 0.1 mmol, 0.2 mmol, 0.3 mmol, 0.5 mmol and 0.6 mmol) dissolved in 5 mL of oleylamine was quickly injected into the solution. The resulting mixture was maintained at 230°C for 30 min. After the solution was cooled to room temperature, the  $Cu_7S_4$  NCs were purified by washing with n-hexane. Subsequently, the  $Cu_7S_4$  NCs dispersed into 15 mL of chloroform for later use.

Synthesis of polymer-modified  $\text{Cu}_7\text{S}_4$  NCs: The asprepared  $\text{Cu}_7\text{S}_4$  NCs were coated with an amphiphilic hydrolyzed poly (maleic anhydride) pre-modified with dodecylamine according to a literature report [23,28]. In a 50 mL round bottom flask, 530 µL of the amphiphilic polymer stock solution (0.8 M monomer units in CHCl<sub>3</sub>), 5 mL of the above  $\text{Cu}_7\text{S}_4$  NCs chloroform solution and 25 mL of anhydrous CHCl<sub>3</sub> were combined and vortexed with magnetically stirring for 45 minutes at room temperature. Subsequent rotary evaporation of the solvent resulted in a dark-brown film of polymer coated  $\text{Cu}_7\text{S}_4$  NCs attached to the inner wall of the flask. 10 mL of aqueous sodium borate buffer (SBB, pH12) was then added to the flask and subject to ultrasonication for 15 min. After phase transfer from chloroform to aqueous solution, the hydrophilic Cu<sub>7</sub>S<sub>4</sub> NCs were collected by centrifugation. The aqueous solution of the Cu<sub>7</sub>S<sub>4</sub> NCs was stored at 4°C for later use.

Measurement of photothermal performance: A 980 nm laser was delivered through a quartz cuvette containing aqueous dispersion (0.3 mL) of the aqueous solution containing Cu<sub>7</sub>S<sub>4</sub>NCs with different concentrations (i.e., 6.25, 12.5, 25, 50, 80, 100 and 150  $\mu$ g/mL). The light source was an external adjustable power (0-0.8 W) 980 nm semiconductor laser device laser module (Xi'an Tours Radium Hirsh Laser Technology Co., Ltd. China). The output power density was independently calibrated to be 0.72 W/cm<sup>2</sup> using a handy optical power meter (Newport model 1918-C, CA, USA). A thermocouple with an accuracy of 0.1°C was inserted into the aqueous dispersion of Cu<sub>7</sub>S<sub>4</sub>NCs, which was oriented perpendicular to the path of the laser beam. The temperature was recorded one time per 5 s.

### In vitro cytotoxicity of $Cu_7S_4$ NCs

Hepatocarcinoma cell lines Hep3B cells were seeded in a 96-well plate at a density of  $1 \times 10^4$  cells/well for 24 h at 37°C in 5%  $\rm CO_2$  to allow the cells to attach. The culture medium was changed and cells were incubated with complete medium containing the  $Cu_7S_4$ NCsat a series of concentrations (i.e., 50, 100, 150, 200 and 250  $\mu$ g/mL) at 37°C with 5% CO<sub>2</sub> for further 24 h. After that, 0.1 mL of 3-(4,5)-dimethylthiahiazo-2vl)-2,5-diphenyltetrazolium bromide (MTT) solution (5 mg/mL, Sigma, Cat.M2003) was added to each well of the microtiter plate and then was incubated in the  $CO_2$ incubator for 4 h. The cells then were lysed by the addition of 100 µL of dimethylsulfoxide (DMSO). The spectrophotometric absorbance of formazan was measured using a plate reader at 570 nm. Four replicates were done for each treatment group.

# In vivo photothermal ablation of cancer cells

Severe combined immunodeficiency (SCID) mice were inoculated subcutaneously with  $4 \times 10^6$  hepatocarcinoma cell lines Hep3B cells on the left side of the rear leg 4-5 weeks before the experiments. When tumors grew to 8-12 mm in diameter, the SCID mice were randomly labeled as control and treatment sample. Two nude mice were first anaesthetized by trichloroacetaldehyde hydrate (10%) at a dosage of 40 mg/kg body weight, and then the treatment and control were injected with 0.15 mL of PBS solution containing the Cu<sub>7</sub>S<sub>4</sub> NCs (150 µg/mL) and saline, respectively, at the central region of the tumors with a depth of  $\sim 4$  mm. After 2 h, the tumors of the control and treatment group were irradiated with 980 nm laser (an output power density of 0.72 W/cm<sup>2</sup>) for 10 min. After that, the two SCID mice were scarified and tumors were removed, embedded in paraffin, and cryosectioned into 4 µm slices. These slides were stained with hematoxylin/eosin, the nexamined under a Zeiss Axiovert 40 CFL inverted fluorescence microscope, and images were captured with a Zeiss AxioCam MRc5 digital camera.

### **Results and discussion**

 $Cu_7S_4$ nanocrystals (NCs) were synthesized by a twostep method, as shown in Fig. 1. As first step, copper nanoparticles were synthesized using oleylamine as reducing agents, according to reported method [25]. Then the as-prepared copper nanoparticles were used as solid precursor, which could react with sulfide source introduced by hot-injection. As a result, the hollowstructure  $Cu_7S_4$  NCs could be successfully fabricated.



Fig. 1 Schematic illustration of the preparation step of  $Cu_7S_4$  NCs with hollow structure.

The copper nanoparticles were prepared without injection of sulfide source (e.g. 0 g). Figure 2(a) showed the typical transmission microscopy (TEM) image of the copper nanoparticles. The particles are spherical and have an average diameter of 15 nm. The high magnification of TEM images (Fig. S1) showed that the copper nanoparticle was crystalline with a certain amount of surface oxidation. As the copper nanoparticle show a high activity to react with oxygen [25], the oxidation likely occurred before XRD measurement when the specimen was exposed to air. Therefore, the crystalline structures of the copper nanoparticles were indexed to CuO (JCPDS card No. 44-0706), as shown in Fig. S3. The resulting UV-vis spectrum of the copper nanoparticles (Fig. S2) exhibited a well-defined surface plasmon absorption peak occurred at around 580 nm, which was consistent with previous reports, confirming the successful synthesis of copper nanoparticles [25].

The resultant copper nanoparticles with a uniform diameter could be used as a sacrificial solid precursor for the synthesis of  $\text{Cu}_7\text{S}_4\text{NCs}$  with hollow structure by injection of an appropriate sulfide source (e.g. 0.6 mmol). Compared to copper seeds synthesized from the first step (Fig. 2(a)), the diameter of  $\text{Cu}_7\text{S}_4$  NCs, after 30 min aging of the second injection of sulfide source, were within an average size of 15-30 nm, as shown in Fig. 2(b). Moreover, the solid nanoparticles were converted into some hollow structures, as shown in high magnification of TEM (Fig. 2(c) and 2(d)). This hollowing process could be explained by the Kirk end all diffusion [26]. The diffraction peaks of the hollow nanoparticles prepared with the S source of 0.6 mmol (Fig. 3) could be indexed with those of  $\text{Cu}_7\text{S}_4$  (JCPDS



Fig. 2 (a) TEM images of copper nanoparticles; ((b), (c) and (d)) TEM and high magnification of TEM images of  $Cu_7S_4$  NCs prepared with the sulfide source of 0.6 mmol.



Fig. 3 XRD of the  $Cu_7S_4$  NCs prepared with different sulfide source (e.g. 0.1 mmol, 0.2 mmol, 0.3 mmol, 0.5 mmol and 0.6 mmol).

card No. 33-0489), confirming the successful preparation of  ${\rm Cu_7S_4}.$ 

Encouragingly, the Cu<sub>7</sub>S<sub>4</sub>NCs dissolved in chloroformshowed an intense absorption band in NIR region owing to the localized surface plasmon resonance (LSPR) mode, as shown in Fig. 4. Specifically, the Cu<sub>7</sub>S<sub>4</sub>NCs exhibit a minimum of absorption around ~670 nm and an increased absorption with the increase of wavelength with the maximum absorption peak of ~1100 nm, in analogy to the reported Cu<sub>2-x</sub>S [19,24]. This stronger absorption in NIR region of Cu<sub>7</sub>S<sub>4</sub> NCs prepared by injecting sulfide source makes them a potential 980 nm-laser-driven photothermal agents for ablation of cancer cells.



Fig. 4 UV-Vis-NIR absorbance spectrum of chloroform solution containing the  $Cu_7S_4$  NCs prepared with the sulfide source of 0.6 mmol.

We also investigated the effect of sulfide amount on crystal structure and morphology of copper sulphide nanoparticles. The resultant copper nanoparticles, as sacrificial templates, were used to react with sulfide source with different doses (e.g. 0.1 mmol, 0.2 mmol, 0.3 mmol and 0.5 mmol). The corresponding X-ray diffraction (XRD) patternswere displayed in Fig. 3. The diffraction peaks of all as-prepared Cu<sub>7</sub>S<sub>4</sub> NCs could be indexed with those of Cu<sub>7</sub>S<sub>4</sub> (JCPDS card No. 33-0489), confirming the successful preparation of Cu<sub>7</sub>S<sub>4</sub>. According to the previous literatures, there are at least five stable phases for the Cu<sub>2-x</sub>S system (i.e., covellite CuS, anilite Cu<sub>1.75</sub>S, digenite Cu<sub>1.8</sub>S, djurlite Cu<sub>1.95</sub>S, and chalcocite Cu<sub>2</sub>S) [19,21,27]. In the present study, we are able to obtain ananilite Cu<sub>7</sub>S<sub>4</sub>



Fig. 5 TEM images and high magnification of TEM of  $Cu_7S_4$  NCs prepared with the sulfide source of ((a), (b)) 0.1 mmol, ((c), (d)) 0.2 mmol, respectively.



Fig. 6 TEM images and high magnification of TEM of  $Cu_7S_4$  NCs prepared with the sulfide source of ((a), (b)) 0.3 mmol, ((c), (d)) 0.5 mmol, respectively.

nanocrystals (orthorhombic, space group P62/nma JCPDS No.33-0489) from Cu nanoparticles by injecting of different doses of sulfide source. It seems that the amount of sulfide source has no obvious effect on the crystal structure of final product. It should also be noted that the difference in morphology and size can be largely dependent on the amount of sulfide source. When adding 0.1 mmol of sulfide source, the obtained nanocrystals with spherical shape and relatively uniform diameter of 25 nm, as shown in Fig. 5(a) and 5(b). With the increase of the sulfide source from 0.1 mmol to 0.2 mmol, the uniformity of size decreased. Specifically, two obvious different sizes (including average diameter 15 and 35 nm) of nanocrystals coexisted in the final product, as shown in Fig. 5(c). Moreover, the nanoparticles exhibit obvious hollow structure, as shown in Fig. 5(d). Further increase of sulfide source to 0.3 mmol resulted in more triangular morphology existing in the product as shown in Fig. 6(a) and 6(b). Besides, 0.5 mmol of sulfide source could lead to less obviously hollow core structure in final products as show in Fig. 6(c) and 6(d).

Due to their strong absorption in NIR region, the  $Cu_7S_4$  NCs prepared with 0.6 mmol of sulfide source were chosen as an example to investigate the photothermal conversion performance and the potential as 980 nm-laser-driven photothermal agents. The assynthesized  $Cu_7S_4$  NCs were passivated with oleylamine and could not be dispersed into aqueous or physiological solution, which limited these nanocrystals applying directly to biological system. To obtain hydrophilic  $Cu_7S_4$  NCs, an amphiphilic polymer was coated on the surface of  $Cu_7S_4$  NCs by hydrophobic self-assembly [23,28]. The polymer-modified  $Cu_7S_4$  NCs could be easily dispersed in water or phosphate buffered saline (PBS) at pH 7.4.

The photothermal conversion performance of the  $Cu_7S_4$  NCs was examined under the irradiation of 980 nm laser with power density of  $0.72 \text{ W/cm}^2$  by detecting the extent of temperature increase, as shown in Fig. 7. Pure water was used as a negative control. The temperatures of all the  $Cu_7S_4$  NCs increased with the irradiation time, and the temperature increased more rapidly with increasing the concentration of  $Cu_7S_4$  NCs. The temperature of  $Cu_7S_4$  NCs aqueous dispersion (e.g.  $150 \ \mu g/mL$ ) could be elevated by 15.7°C with the irritation of 980 nm laser for 400 s, compared with pure water (i.e.,  $0 \,\mu g/mL$ ) that was only increased by less than  $4^{\circ}$ C. These confirmed the Cu<sub>7</sub>S<sub>4</sub> NCs can rapidly and efficiently convert the 980 nmlaser energy into thermal energy. Moreover, with the increase of the concentration (i.e., from 6.25 to 12.5, 25, 50, 80 and 100  $\mu g/mL$ ), the temperature of the Cu<sub>7</sub>S<sub>4</sub> NCs aqueous dispersion could be increased by 6.5, 8, 8.7, 10.1, 12.2 and 14.1°C, respectively (Fig. 7(b)). As is well-known, hyperthermic therapy takes advantage of heat between 40 and  $45^{\circ}$ C to damage cancer cells [29]. Assuming that the temperature of *in vivo* human body is 37°C, tumor region injected with an aqueous dispersion of  $Cu_7S_4$  NCs can easily be heated to over  $45^{\circ}C$ within 400 s by irradiation with a 980 nm laser (0.72  $W/cm^2$ ), which probably efficiently induces cancer cells death [29].

The influence of the  $Cu_7S_4$  NCs on the viabilities of cancer cells were used to evaluate the biocompatibility



Fig. 7 Temperature elevation of the aqueous solution containing  $Cu_7S_4$  NCs with different concentrations (i.e., 6.25, 12.5, 25, 50, 80, 100 and 150 µg/mL) as a function of time (0-400 s) under the irradiation of 980 nm laser with power density of 0.72 W/cm<sup>2</sup>; (b) Plot of temperature change over a period of 400 s versus the aqueous dispersion of the  $Cu_7S_4$  NCs.

in vitro. The Cu<sub>7</sub>S<sub>4</sub> NCs with various concentrations (i.e., 50, 100, 150, 200 and 250  $\mu$ g/mL) were incubated with Hepatocarcinoma cell lines Hep3B cells for 24 h and then the cell viabilities were tested by using the 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT) assay. There was no obvious adverse effect on cell viabilities, even the concentration reaching 250  $\mu$ g/mL, as shown in Fig. 8, which meant a low cytotoxicity induced by Cu<sub>7</sub>S<sub>4</sub> NCs.



Fig. 8 The viabilities of Hep3B cells incubated with the Cu<sub>7</sub>S<sub>4</sub> NCs with different concentrations (i.e., 50, 100, 150, 200 and 250  $\mu$ g/mL) for 24 h, measured by MTT assay. Data represents the mean±standard deviation of four experiments.

To evaluate photothermal ablation effect of cancer cells, two nude mice bearing evident tumors were randomly divided into control and treatment group. The control mouse was injected with 200  $\mu$ L of saline in the central region of the tumor, while the treatment mouse was injected with 200  $\mu$ L of PBS containing Cu<sub>7</sub>S<sub>4</sub> NCs (e.g., 150  $\mu$ g/mL). After 2 h, the tumors of the two mice were irradiated with 980 nm of laser for 10 min (see detail in experiment section and the experimental setup shown in Fig. S4). Subsequently, PTA effects of tumor tissues in mice were confirmed by histological examination (hematoxylin/eosin (H&E) staining), as shown in Fig. 9. In the case of control group, there were little change regarding the cells' sizes and shapes, nuclear modifications as shown in Fig. 9(a) and 9(c). In the case of treatment group, under the same irradiation conditions, the common signs of thermal cell necrosis are presented on considerable regions of the examined tumor slide (Fig. 9(b)). Furthermore, more destruction of the tumor cells, such as shrinkage of the malignant cells, loss of contact, eosinophilic cytoplasm, and nuclear damage could be observed from Fig. 9(d). These facts suggested that in vivo cancer cells could be efficiently destroyed by the high temperature arising from the excellent photothermal effect of Cu<sub>7</sub>S<sub>4</sub> NCs. Therefore, it is safe to conclude that Cu<sub>7</sub>S<sub>4</sub> NCs have great potential to be used as an excellent photothermal agent for PTA therapy.

#### Conclusion

Using the copper nanoparticles as a starting precursor, we have successfully synthesized  $\text{Cu}_7\text{S}_4$  NCs with hollow structure, which exhibited intense absorption band at NIR wavelengths due to LSPR. The hydrophilic  $\text{Cu}_7\text{S}_4$  NCs coated with amphiphilic polymer could effectively convert 980 nm-laserenergy into heat and further destroy cancel cells *in vivo*. Therefore, these  $\text{Cu}_7\text{S}_4$ hollow NCs demonstrated great superiority as an excellently potential photothermal agent, as a result of their small size and high photothermal conversion efficiency as well as their low cost.

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Fig. 9 (a)-(d) Representative H&E stained histological images of *in vivo* tumor sections treated by the irradiation of 980 nm laser (0.72 W/cm<sup>2</sup>) over a period of 10 min injected with ((a), (c)) saline and ((b), (d)) PBS solution of the Cu<sub>7</sub>S<sub>4</sub> NCs (150  $\mu$ g/mL), respectively.

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